

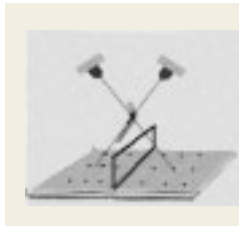
# RADIOSTEREOMETRIC ANALYSIS (RSA) STUDIES AT MASSACHUSETTS GENERAL HOSPITAL

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## INTRODUCTION

Radiostereometric analysis (RSA) was developed by Selvik *et al.* as a method for performing very accurate three-dimensional measurements *in vivo* over time from sequential radiographs<sup>37,38</sup>. This technique has been used for over twenty years to assess growth plate integrity<sup>1,10-12,15,18-20,35</sup>, total joint replacement implant stability<sup>24,25,27,36,39</sup>, spinal fusion stability<sup>16,17,34</sup>, as well as in kinematic studies of the knee, spine, and shoulder<sup>3,13,14,22,23,26,28,29,31-33,36,42</sup>.



**Figure 1.** Schematic drawing of the radiographic set up used for obtaining the pair of radiographs. The region of interest is placed in front of the calibration cage at the point where the two x-ray beams cross.

The RSA method utilizes dual simultaneous radiographs in conjunction with a calibration cage. The calibration cage contains a number of 1.0mm tantalum beads held in fixed, well-defined positions which allows construction of a three-dimensional coordinate system. Additional tantalum bead markers are placed in the body segments to be studied. A pair of radiographs is taken with the patient in front of the cage with the x-ray sources positioned at an approximately forty degree angle (Figure 1). Analyzing the radiographic film pairs using an interactive software package, the three-dimensional position of each *in vivo* marker can be calculated and then each group of markers is treated as a three-dimensional rigid body segment. Relative displacements between two segments can then be calculated from sequential pairs of radiographs.

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**Figure 2.** The hip phantom allows three dimensional displacements of the femoral head within the acetabular component.



## EXPERIMENTAL HIP PHANTOM STUDIES

Due to its high accuracy, RSA is considered the best technique for measuring femoral head penetration into polyethylene acetabular components *in vivo*. This penetration is a result of both plastic deformation of the polyethylene component as well as the wear of the material occurring at the articulation. However, due to the many variable parameters which can affect the outcome of an RSA study, a physical model which could be used to evaluate these parameters individually is needed. We have developed a phantom total hip replacement model in order to quantify the accuracy and precision of RSA and used it to evaluate methods of bead placement, radiographic methods, as well as to evaluate two commonly used RSA software packages<sup>9</sup>. The hip phantom is shown in Figure 2.

Femoral head penetration can be simulated by moving the femoral head accurately in each plane in discrete increments. Five image pairs were taken before any motion occurred. Motion was first performed in the medial direction, moving 50 $\mu$ m, 100 $\mu$ m, 150 $\mu$ m and finally 200 $\mu$ m into the acetabular component, followed by sequential posterior displacement of 50 $\mu$ m, 100 $\mu$ m, 150 $\mu$ m and 200 $\mu$ m, and thereafter followed by sequential motion in the superior direction using the same distances of 50 $\mu$ m, 100 $\mu$ m, 150 $\mu$ m and 200 $\mu$ m. This group of displacements represents one data set of the phantom. In order to calculate accuracy and precision, five data sets were created.

Using this phantom, we have shown that the *accuracy* of the radiostereometric analysis in this optimal experimental set-up was 33 $\mu$ m for the medial direction, 22 $\mu$ m for the superior direction, 86 $\mu$ m for the posterior direction, and 55 $\mu$ m for the resultant three-dimensional vector length. The corresponding *precision* at the 95% confidence interval measured 8.4 $\mu$ m for the medial direction, 5.5 $\mu$ m for the superior direction, 16.0 $\mu$ m for the posterior direction and 13.5 $\mu$ m for the resultant three-dimensional vector length<sup>9</sup>.

We have also compared the use of conventional plain radiographs to digital DICOM images. The accuracy and precision values resulting from the analysis of the digital films were consistently better than that resulting from the use of

the conventional films. For both the conventional and digital radiographic methods, the poorest accuracy and precision values were for the posterior, out-of-plane vector.

There are two widely used software packages that have been developed for RSA analysis: the UmRSA™ package developed by Biomedical Innovations AB, Umeå, Sweden<sup>7,21</sup>, and the RSA-CMS, (RSA Clinical Measurement Solution) developed at the University of Leiden, The Netherlands<sup>2,41</sup>. The accuracy and precision using the two different software systems was evaluated by using the same five sets of digital examinations. The accuracy values resulting from the RSA-CMS™ analysis were two times worse than those resulting from the analysis of the same films using the UmRSA™ software<sup>8</sup>.

Finally, we have evaluated two different methods for marking the acetabular component in preparation for a clinical study. We used specially designed towers secured to the metal shell to hold the tantalum beads as well as placing a series of beads into the peripheral flange of the polyethylene insert. We found that there was no significant difference in the data resulting from the two different configurations of the tantalum markers<sup>8</sup>.

### CLINICAL STUDIES

The first clinical studies using RSA in North America have been initiated at Massachusetts General Hospital. Two studies are underway which are designed to evaluate the *in vivo* wear performance of a new form of highly crosslinked polyethylene acetabular component used in total hip replacement surgery. Each study has two patient groups. One group receives highly crosslinked acetabular components in conjunction with a 28mm cobalt chrome femoral head. The other group receives



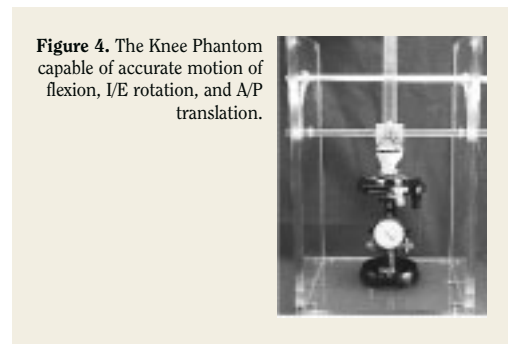
highly crosslinked acetabular components coupled with larger diameter femoral heads (36mm or 38mm) than have been routinely used in the past. These studies are designed to follow the groups of patients over a period of five years. An example of a RSA clinical radiograph is shown in Figure 3.

### EXPERIMENTAL KNEE KINEMATIC STUDIES

Knee kinematics following total knee replacement surgery is dependant in large measure on the design of the implants. Some knee components are designed to limit anterior/posterior translation and rotation. Others are designed to enhance mobility and increase the amount of functional knee flexion. Moreover, the resulting kinematics for a particular implant design are known to be quite variable among patients. Many efforts have been made to develop techniques to measure knee kinematics *in vivo* more accurately. Two approaches have been

widely used: one uses radiographic images obtained with fluoroscopy and calculates three dimensional relative motion by matching the projected profile of the implant with the computerized implant geometry.<sup>4-6,30</sup> The other uses RSA to calculate relative displacements from a series of radiographic film pairs<sup>22,28,29,40</sup>. To date, no standardized method has been developed to judge the accuracy of these techniques for measuring knee joint kinematics.

We have developed an *in vitro* model of a total knee replacement which is capable of accurate three-dimensional motions. With this model, we have begun to evaluate the RSA method of measuring knee joint kinematics. The knee phantom model was constructed using NK-II femoral and tibial components (Centerpulse Orthopaedics, Austin, TX). A mock left femur was machined from Plexiglas with the appropriately machined cuts to receive a size three left femoral component. The distal femur was held in a separate Plexiglas frame by passing a half-inch Plexiglas dowel thru the hole in the distal femur. Flexion/extension of the femur occurred around the half-inch dowel. The femoral construct could be fixed at any angle of flexion by fixation to the surrounding frame. A digital inclinometer, accurate to 0.1°, was used to measure the flexion angle relative to full extension. A sawbones proximal tibia was used to hold the tibial component. This was secured to a rotary table with rotation which was accurate to 1.0 degree. This in turn was mounted to an x, y, z table in order to control the proximal/distal positioning of the tibia and anterior/posterior translation (Figure 4). Motions in the medial/lateral plane and



medial/lateral tilt were not simulated. A displacement protocol was developed to simulate flexion of the knee from full extension to 75° of flexion and back to neutral in twelve steps, while simultaneously simulating the internal/external rotation, and anterior/posterior translation.

For RSA evaluation, 1.0mm tantalum markers were placed in the distal femur, the proximal tibia and the side of the polyethylene liner. Simultaneous radio-pairs were obtained for each of the twelve displacements using the RSA cage, and the RSA analysis was performed using the UmRSA Biomedical software package. Relative displacements were calculated by using the first film pair as the reference. The error was calculated by subtracting the value measured by RSA from the actual known displacement.

There was good agreement between the actual displacement and the measurements of displacements measured by RSA for flexion, rotation and translation. For flexion, the error values ranged from 0.05 - 1.85 degrees, resulting in an average flexion error of  $0.78 \pm 0.95$  degrees. For internal/external rotation, the error values ranged from 0.15 - 0.92 degrees resulting in an average rotational error of  $0.52 \pm 0.30$  degrees. Finally, for the translation, the error values ranged from 0.29 – 2.0 millimeters resulting in an average translation error of  $0.37 \pm 1.26$  millimeters.

#### **SUMMARY**

Radiostereometric analysis (RSA) is a powerful tool for clinical assessment. The initial focus of our studies has been to assess the performance of two designs of acetabular implants which utilize a newly developed highly crosslinked polyethylene. Likewise, the use of this new polyethylene in total knee

arthroplasty may allow for innovative designs to be introduced for clinical use. These types of early clinical follow-up studies are a critical part of evidence-based medicine when new materials or implant designs are introduced for clinical use. Also important in clinical analysis are joint kinematic studies as well as implant stability studies using RSA. In order to address this a physical knee phantom for assessing various methods of measuring knee joint kinematics has been developed.

Our preliminary study has shown good agreement between the actual displacements of the knee phantom and that measured from radiographic pairs using RSA. Our results show the marker configuration used in this study appears to be adequate for kinematic analysis in a clinical setting. Finally, the capacity of performing RSA studies following spinal surgery, shoulder arthroplasty, and other orthopaedic procedures is now possible.



Don Bae, Jeannie Chung, Courtney Gobezie, and Reuben Gobezie dining at the thesis day awards dinner.

## References

1. **Alberius, P., and Selvik, G.:** Roentgen stereophotogrammetric analysis of growth at cranial valve sutures in the rabbit. *Acta-Anat-Basel*, 117(2): 170-80, 1983.
2. **Alfaro-Adrian, J.; Gill, H. S.; and Murray, D. W.:** Cement migration after THR. A comparison of charnley elite and exeter femoral stems using RSA. *Journal of Bone & Joint Surgery - British Volume*, 81(1): 130-4, 1999.
3. **Axelsson, P.; Johnsson, R.; and Strömqvist, B.:** The spondylyolytic vertebra and its adjacent segment. Mobility measured before and after posterolateral fusion. *Spine*, 22(4): 414-7, 1997.
4. **Banks, S. A., and Hodge, W. A.:** Accurate measurement of three-dimensional knee replacement kinematics using single-plane fluoroscopy. *IEEE Transactions on Biomedical Engineering*, 43(6): 638-49, 1996.
5. **Banks, S. A.; Markovich, G. D.; and Hodge, W. A.:** In vivo kinematics of cruciate-retaining and -substituting knee arthroplasties. *Journal of Arthroplasty*, 12(3): 297-304, 1997.
6. **Bellemans, J.; Banks, S.; Victor, J.; Vandenneucker, H.; and Moemans, A.:** Fluoroscopic analysis of the kinematics of deep flexion in total knee arthroplasty. Influence of posterior condylar offset. *Journal of Bone & Joint Surgery - British Volume*, 84(1): 50-3, 2002.
7. **Börlin, N.; Thien, T.; and Kärrholm, J.:** The Precision of Radiostereometric Measurements. Manual vs. Digital Measurements. *Journal of Biomechanics*: Submitted, 2001.
8. **Bragdon, C. E., D. M.; Veldhoven, J.; Yuan, X.; Bourne, R.; Malchau, H.; Kärrholm, J.; Harris, W.H.:** Validation of the use of Digital Radiography for Radiostereometric Analysis of THR Wear and an Evaluation of Two RSA Software Systems Using A Phantom Model. In *European Orthopaedic Research Society*, pp. 069. Edited by Leyvraz, P., Quinn, Zysset, 069, Lausanne, Switzerland, 2002.
9. **Bragdon, C. R.; Malchau, H.; Yuan, X.; Perinchief, R.; Kärrholm, J.; Borlin, N.; Estok, D. M.; and Harris, W. H.:** Experimental assessment of precision and accuracy of radiostereometric analysis for the determination of polyethylene wear in a total hip replacement model. *Journal of Orthopaedic Research*, 20(4): 688-95, 2002.
10. **Bylander, B.; Aronson, S.; Egund, N.; Hansson, L. I.; and Selvik, G.:** Growth disturbance after physial injury of distal femur and proximal tibia studied by roentgen stereophotogrammetry. *Arch-Orthop-Trauma-Surg.*, 98(3): 225-35, 1981.
11. **Bylander, B.; Hansson, L. I.; and Selvik, G.:** Pattern of growth retardation after Blount stapling: a roentgen stereophotogrammetric analysis. *J-Pediatr-Orthop.*, 3(1): 63-72, 1983.
12. **Bylander, B.; Selvik, G.; Hansson, L. I.; and Aronson, S.:** A roentgen stereophotogrammetric analysis of growth arrest by stapling. *J-Pediatr-Orthop.*, 1(1): 81-90, 1981.
13. **Dickman, C. A.; Crawford, N. R.; and Paramore, C. G.:** Biomechanical characteristics of C1-2 cable fixations. *J-Neurosurg.*, 85(2): 316-22, 1996.
14. **Fuller, D. A.; Kirkpatrick, J. S.; Emery, S. E.; Wilber, R. G.; and Davy, D. T.:** A kinematic study of the cervical spine before and after segmental arthrodesis. *Spine*, 23(15): 1649-56, 1998.
15. **Hägglund, G.; Bylander, B.; Hansson, L. I.; Kärrholm, J.; Selvik, G.; and Svensson, K.:** Longitudinal growth of the distal fibula in children with slipped capital femoral epiphysis. *J-Pediatr-Orthop.*, 6(3): 274-7, 1986.
16. **Johnsson, R.; Axelsson, P.; and Strömqvist, B.:** Posterolateral lumbar fusion using facet joint fixation with biodegradable rods: a pilot study. *Eur-Spine-J.*, 6(2): 144-8, 1997.
17. **Johnsson, R.; Selvik, G.; Strömqvist, B.; and Sundén, G.:** Mobility of the lower lumbar spine after posterolateral fusion determined by roentgen stereophotogrammetric analysis. *Spine*, 15(5): 347-50, 1990.
18. **Kärrholm, J.; Hansson, L. I.; and Selvik, G.:** Longitudinal growth rate of the distal tibia and fibula in children. *Clinical Orthopaedics & Related Research*, (191): 121-8, 1984.
19. **Kärrholm, J.; Hansson, L. I.; and Selvik, G.:** Roentgen stereophotogrammetric analysis of growth pattern after pronation ankle injuries in children. *Acta-Orthop-Scand.*, 53(6): 1001-11, 1982.
20. **Kärrholm, J.; Hansson, L. I.; and Selvik, G.:** Roentgen stereophotogrammetric analysis of growth pattern after supination-adduction ankle injuries in children. *J-Pediatr-Orthop.*, 2(3): 271-9, 1982.
21. **Kärrholm, J.; Herberts, P.; Hultmark, P.; Malchau, H.; Nivbrant, B.; and Thanner, J.:** Radiostereometry of hip prostheses. Review of methodology and clinical results. *Clin Orthop*, (344): 94-110, 1997.
22. **Kärrholm, J.; Jonsson, H.; Nilsson, K. G.; and Soderqvist, I.:** Kinematics of successful knee prostheses during weight-bearing: three-dimensional movements and positions of screw axes in the Tricon-M and Miller-Galante designs. *Knee-Surg-Sports-Traumatol-Arthrosc.*, 2(1): 50-9, 1994.
23. **Lee, S.; Harris, K. G.; Nassif, J.; Goel, V. K.; and Clark, C. R.:** In vivo kinematics of the cervical spine. Part I: Development of a roentgen stereophotogrammetric technique using metallic markers and assessment of its accuracy. *J-Spinal-Disord.*, 6(6): 522-34, 1993.
24. **Linder, L.:** Implant stability, histology, RSA and wear—more critical questions are needed. A view point. *Acta Orthop Scand*, 65(6): 654-8, 1994.
25. **Lippert, F. G. d.; Harrington, R. M.; Veress, S. A.; Fraser, C.; Green, D.; and Bahniuk, E.:** A comparison of convergent and bi-plane X-ray photogrammetry systems used to detect total joint loosening. *J Biomech*, 15(9): 677-82, 1982.
26. **Nagels, J.; Valstar, E. R.; Stokdijk, M.; and Rozing, P. M.:** Patterns of loosening of the glenoid component. *Journal of Bone & Joint Surgery - British Volume*, 84(1): 83-7, 2002.
27. **Nilsson, K. G., and Dalén, T.:** Inferior performance of Boneloc bone cement in total knee arthroplasty: a prospective randomized study comparing Boneloc with Palacos using radiostereometry (RSA) in 19 patients. *Acta Orthop Scand*, 69(5): 479-83, 1998.
28. **Nilsson, K. G.; Kärrholm, J.; and Ekelund, L.:** Knee motion in total knee arthroplasty. A roentgen stereophotogrammetric analysis of the kinematics of the Tricon-M knee prosthesis. *Clin-Orthop.*, (256): 147-61, 1990.
29. **Nilsson, K. G.; Kärrholm, J.; and Gadegaard, P.:** Abnormal kinematics of the artificial knee. Roentgen stereophotogrammetric analysis of 10 Miller-Galante and five New Jersey LCS knees. *Acta-Orthop-Scand.*, 62(5): 440-6, 1991.
30. **Nozaki, H.; Banks, S. A.; Suguro, T.; and Hodge, W. A.:** Observations of femoral rollback in cruciate-retaining knee arthroplasty. *Clinical Orthopaedics & Related Research*, (404): 308-14, 2002.
31. **Olin, T.; Olsson, T. H.; Selvik, G.; and Willner, S.:** Kinematic analysis of experimentally provoked scoliosis in pigs with Roentgen stereophotogrammetry. *Acta-Radiol-Diagn-Stockh.*, 1F(1): 107-27, 1976.
32. **Olsson, T. H.; Selvik, G.; and Willner, S.:** Kinematic analysis of posterior spinal fusions in pigs. *Acta-Radiol-Diagn-Stockh.*, 17(3): 369-84, 1976.
33. **Olsson, T. H.; Selvik, G.; and Willner, S.:** Kinematic analysis of posterolateral fusion in the lumbosacral spine. *Acta-Radiol-Diagn-Stockh.*, 17(4): 519-30, 1976.
34. **Olsson, T. H.; Selvik, G.; and Willner, S.:** Mobility in the lumbosacral spine after fusion studied with the aid of roentgen stereophotogrammetry. *Clin-Orthop.*, (129): 181-90, 1977.
35. **Rune, B.; Sarnas, K. V.; Selvik, G.; and Jacobsson, S.:** Movement of the cleft maxilla in infants relative to the frontal bone. A roentgen stereophotogrammetric study with the aid of metallic implants. *Cleft-Palate-J.*, 17(2): 155-74, 1980.
36. **Selvik, G.:** Roentgen stereophotogrammetric analysis. *Acta-Radiol.*, 31(2): 113-26, 1990.
37. **Selvik, G.:** A stereophotogrammetric system for the study of human movements. *Scand-J-Rehabil-Med-Suppl.*, 6: 16-20, 1978.
38. **Selvik, G.; Alberius, P.; and Aronson, A. S.:** A roentgen stereophotogrammetric system. Construction, calibration and technical accuracy. *Acta-Radiol-Diagn-Stockh.*, 24(4): 343-52, 1983.
39. **Thanner, J.; Kärrholm, J.; Malchau, H.; Wallinder, L.; and Herberts, P.:** Migration of press-fit cups fixed with poly-L-lactic acid or titanium screws: a randomized study using radiostereometry. *J Orthop Res*, 14(6): 895-900, 1996.
40. **Uvehammer J, K. J., Brandsson S, Herberts P, Carlsson L, Karlsson J, Regné L.:** In vivo kinematics of total knee arthroplasty. Flat vs. concave tibial joint surface. *J Orthop Res*: in press, 2001.
41. **Valstar, E. R.:** Digital Roentgen Stereophotogrammetry. Development, Validation, and Clinical Application. *Thesis, University of Leiden, Leiden, Holland*, ISBN 90-9014397-1, NUGI 743, 2001.
42. **Weidenhielm, L.; Wykman, A.; Lundberg, A.; and Brostrom, L. A.:** Knee motion after tibial osteotomy for arthrosis. Kinematic analysis of 7 patients. *Acta-Orthop-Scand.*, 64(3): 317-9, 1993.